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APPARATUS AND METHOD FOR THE MEASUREMENT AND ASSESSMENT OF
SLING-TENSION FOR TREATMENT OF FEMALE URINARY INCONTINENCE ;

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ABSTRACT:

A urinary apparatus includes a catheter system for pressurizing either a bladder cavity or a urethral canal within a female urinary system and an endoscope device for observing a urethral sphincter muscle within the female urinary system for assessing the sling tension of an implant support adapted to restore female urinary continence. The catheter system includes a obturator occlusion member for plugging the urethral canal during the performance of a sling tensioning procedure

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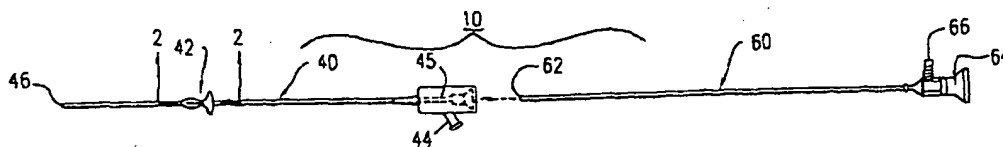
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(54) Title: APPARATUS AND METHOD FOR MEASUREMENT AND ASSESSMENT OF SLING-TENSION FOR TREATMENT OF FEMALE URINARY INCONTINENCE



(57) Abstract: A urinary apparatus includes a catheter system for pressurizing either a bladder cavity or a urethral canal within a female urinary system and an endoscope device for observing a urethral sphincter muscle within the female urinary system for assessing the sling tension of an implant support adapted to restore female urinary continence. The catheter system includes an obturator occlusion member for plugging the urethral canal during the performance of a sling tensioning procedure.

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APPARATUS AND METHOD FOR THE MEASUREMENT AND ASSESSMENT OF SLING-TENSION FOR TREATMENT OF FEMALE URINARY INCONTINENCE

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Cross Reference To Related Applications

This is a § 111(a) application relating to a Provisional U.S. Appln. Serial No. 60/242,554 filed October 23, 2000.

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Field Of The Invention

The present invention relates generally to a surgical urinary instrument and a method for treating female urinary incontinence. More particularly, the apparatus and method can be utilized to assess the efficacy of an implant which is adapted to support the urethral sphincter muscle of the bladder for the purpose of restoring continence.

20 Background Of The Invention

Women account for more than 11 million of incontinence cases. Moreover, a majority of women with incontinence suffer from stress urinary incontinence (SUI). Women with SUI involuntarily lose urine during normal daily activities and movements, such as laughing, coughing, sneezing and regular exercise.

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SUI may be caused by a functional defect of the tissue or ligaments connecting the vaginal wall with the pelvic muscles and pubic bone. Common causes include repetitive straining of the pelvic muscles, childbirth, loss of pelvic muscle tone and estrogen loss. Such a defect results in an improperly functioning urethra. Unlike other types of incontinence, SUI is not a problem of the bladder.

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Normally, the urethra, when properly supported by strong pelvic floor muscles and healthy connective tissue, maintains a tight seal to prevent involuntary loss of urine. When a woman suffers from the most common form of SUI, however, weakened muscle and pelvic tissues are unable to adequately support the urethra in its correct position. As a result, during normal movements when pressure is exerted on the bladder from the diaphragm, the urethra cannot retain its seal, permitting urine to escape. Because SUI is both embarrassing and unpredictable, many women with SUI avoid an active lifestyle, shying away from social situations.

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In an effort to help manage female SUI, a physician may surgically place a supportive implant to raise the bladder neck and restore continence. These

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surgical devices, which are commonly referred to as "slings", are placed in-vivo in a number of ways.

United States Patent No. 5,112,344 describes a method and apparatus for treating female incontinence. The surgical instrument for the application of a
5 filamentary element into the body comprises a tubular shaft having a handle at one end and a flexible needle slidably receivable in the shaft and adapted at one end to receive a filamentary element. The method of treating female incontinence comprises the steps of (1) looping the filamentary element between the wall of the vagina and the rectus abdominis sheath in the anterior wall of the abdomen, whereby
10 the filamentary element passes to each side of the urethra; (2) adjusting the loop to bring the vaginal wall and the urethra into the correct spatial relationship to the pubis, thereby allowing the development of scar tissue between the vaginal wall and the anterior wall of the abdomen pubic symphysis; and (3) removing the filamentary element.

15 United States Patent No. 5,899,909 discloses a surgical instrument comprising a shank having a handle at one end and connecting means at the other end to receive a pair of curved needles. In practice, a first needle is connected to one end of a tape, while a second needle is connected to an opposite end of the tape. The first needle is then passed into the body via the vagina, through the
20 vaginal wall, and past one side of the urethra. The first needle is then further passed over the pubis and through the abdominal wall, thereby drawing the end of the tape through the body along one side of the urethra. The second needle is also passed into the body via the vagina, through the vaginal wall, and past an opposite side of the urethra. The second needle is then further passed over the pubis and through
25 the abdominal wall, thereby drawing the opposite end of the tape through the body along an opposite side of the urethra, such that the tape forms a loop about the urethra. After the tape is extended over the pubis and through the abdominal wall, it is tightened. The tape ends are then cut at the abdominal wall, leaving the tape implanted in the body.

30 After placing the sling in the patient, the physician positions the sling with respect to the bladder and urethra. The position required to restore continence is individually determined for each patient by the surgeon. One method to position

the sling is to provide the bladder with a predetermined stress or pressure and then the sling is positioned until continence is restored. The stress or pressure applied to the bladder may be provided in two different ways.

If the patient is awake, the physician may instruct the patient to apply
5 abdominal pressure via muscle contraction, such as by coughing. This naturally applied force is considered to be the best gauge for "natural" continence evaluation. However, having the patient awake for this portion of the procedure is clinically inconvenient.

The second method is the most widely used procedure both
10 domestically and internationally. Since the patient is typically anesthetized, requesting the patient to cough or pressurize the bladder is not possible. Consequently, the physician may apply firm positive pressure to the anterior pelvic portion of the body in an effort to induce micturition (i.e., the act of urinating). Pressure is applied repeatedly while the tape or sling is adjusted. The tape is
15 adjusted until only a minor trace of the fluid flow exits the urethra.

When a patient is under general anesthesia and in the supine position, abdominal and skeletal retention muscles are inactive. When manual pressure is applied as in the aforementioned manner, it is believed that the force/pressure focused on the bladder is actually dissipated by the overall relaxed state of the lower
20 abdomen. Gauging tape position and subsequent urodynamics in this manner is extremely dangerous and can lead to adverse conditions, such as urethral restriction, or may maintain incontinence.

Thus, there is a need for an apparatus and method for measuring and monitoring urodynamic flow and pressure variations while positioning the tape in
25 such a way to provide the physician with the exact information needed to ensure optimal clinical safety and efficacy of the tape, as demonstrated by the urinary apparatus of the present invention.

The present invention overcomes the deficiencies of the prior art and provides for an improved urodynamic measurement system that may be used in
30 conjunction with any procedure to treat SUI such as those to suspend the bladder neck or support the urethral sphincter muscle. For illustrative purposes only, the present invention will be discussed in combination with the apparatus and method

disclosed in the aforementioned U.S. Patent No. 5,899,909, which is incorporated herein by reference.

Summary Of The Invention

5 In accordance with one aspect of the present invention, a urinary apparatus for assessing the sling tension of an implant support for restoring female urinary continence includes a catheter system for pressurizing either a bladder cavity or a urethral canal within a female urinary system. The urinary apparatus also includes an endoscope device for observing a urethral sphincter muscle within the
10 female urinary system for assessing the sling tension of the implant support, such as a tension-free vaginal tape. The catheter system includes an obturator occlusion member for plugging the urethral canal in order to pressurize the bladder cavity and the urethral canal during the performance of a sling tensioning procedure which includes the steps of: pressurizing the bladder cavity with fluid to a predetermined
15 pressure; pressurizing the urethral canal with fluid to a pressure level at which the urethral sphincter muscle opens so as to induce reverse leakage back into the bladder; observing the opening of the urethral sphincter muscle during the performance of the preceding step; and adjusting the sling tension of the implant support in response to the pressure level achieved during the pressurization of the
20 urethral canal.

Brief Description Of The Drawings

Further objects, features and advantages of the present invention will become apparent upon consideration of the following detailed description of various
25 exemplary embodiments considered in conjunction with the accompanying drawings, in which:

Figure 1 is an exploded elevational view of a urinary apparatus constructed in accordance with one exemplary embodiment of the present invention;

Figure 2 is an enlarged cross-sectional view of the urinary apparatus of Figure 1 taken along section line 2-2 and looking in the direction of the arrows;

Figure 3 is a schematic view of a female urinary/reproductive system and the urinary apparatus of Figure 1, showing a tip portion of the urinary apparatus
5 being inserted into a urethra canal;

Figure 4 is a view similar to the view of Figure 3, except that the tip portion of the urinary apparatus is shown in contact with an internal urethral sphincter muscle;

Figure 5 is a view similar to the view of Figure 4, except that the tip
10 portion of the urinary apparatus is shown within the lower urethra canal and a slidable obturator occlusion plug is blocking the opening of the urethra canal;

Figure 6 is a view similar to the view of Figure 5, except that the urinary apparatus has a pressure gauge, a syringe and a video monitor attached thereto;

Figure 7a is a schematic view of the video monitor of the urinary
15 apparatus of Figure 6 showing the urethral sphincter muscle in a non-functional orientation;

Figure 7b is a schematic view of the video monitor of the urinary
apparatus of Figure 6 showing the urethral sphincter muscle in a completely closed
20 position;

Figure 7c is a schematic view of the video monitor of the urinary
apparatus of Figure 6 showing the urethral sphincter muscle in a normal and
functional orientation;

Figure 8 is a front elevational view of the urinary apparatus of Figure
25 6 showing an electronic pressure gauge attached to the occlusion catheter;

Figure 9 is a front elevational view of a fixed balloon occlusion catheter constructed in accordance with another exemplary embodiment of the present invention;

Figure 10 is an enlarged cross-sectional view of the fixed balloon
30 occlusion catheter of Figure 9 taken along section line 10-10 and looking in the direction of the arrows; and

Figure 11 is a front elevational view of a sliding balloon occlusion catheter constructed in accordance with yet another exemplary embodiment of the present invention.

5 Detailed Description Of The Exemplary Embodiments

With reference generally to Figures 1 through 6, a urinary apparatus 10 is shown which is adapted to be received within a human female urinary system 12. In order to fully understand the advantages of the urinary apparatus 10, a brief overview of the female urinary system 12 is discussed below with particular
10 reference to Figure 3.

The female urinary system 12 includes an elongated urethral canal 14 having a substantially circular-shaped urethral sphincter muscle 16 attached thereto, and a bladder cavity 18 surrounded by a detrusor muscle 20. The detrusor muscle 20 also surrounds and supports the urethral canal 14. The bladder cavity 18 is in
15 close proximity to the abdominal wall 22, the pubic bone 24, the pelvic floor 26 (levator ani muscle), the vaginal canal 28 and the uterus 30, as depicted in Figure 3.

Referring again to Figures 1 through 6, the urinary apparatus 10 includes a slender and flexible catheter system 40 having a slidable obturator
20 occlusion (plug) member 42 thereon; and a small diameter and flexible endoscope device 60 slidably received within the catheter system 40. The plug member 42 is sized and shaped to fit an entrance opening 14a of the urethral canal 14 and is made from a solid, pliable plastic material. The catheter system 40 has a proximal end which includes an inlet fill port 44 for receiving a fluid, and a distal end which includes
25 a catheter tip section 46 for discharging fluid. The fill port 44 is detachably connected to a pressure gauge 48 and to a syringe member 50. The syringe member 50 contains the fluid for pressurizing the bladder cavity 18 during the assessment procedures for the sling-tension in the treatment of female incontinence, as will be described more fully hereinafter. With reference to Figure 8, an alternative
30 pressure/measurement device in the form of a urodynamic electronic pressure monitor 52 is used in place of the pressure gauge 48 shown in Figure 6.

With reference to Figures 1 and 3, the endoscope device 60 has a distal end which includes a tip section 62 that can be placed transurethrally, such that the tip section 62 is positioned within the urethral canal 14 of the urinary system 12. The endoscope device 60 also has a proximal end which includes an eye-scope member 64 for viewing in-vivo the urethral canal 14 by the physician (see Figure 3) and an inlet port 66 for receiving another element such as a light source (i.e., a fiber optic light strand - not shown). The endoscope device 60 can be constructed in accordance with the teachings of co-pending, co-owned U.S. Patent Application Serial No. 09/752,259, filed December 29, 2000, which application is incorporated herein by reference.

The endoscope device 60 also includes a video-monitoring scope member 68 for detachably connecting to the eye-scope member 64. The video-monitoring scope member 68 is electronically connected to a video monitor 70 via an electrical line 72 for visually monitoring in-vivo the urethral canal 14 by the medical staff for the assessment and condition of the urethral sphincter muscle 16. This assessment is relative to the tensioning of an inserted tension-free vaginal (mesh) tape (TVT) 74 around the urethral sphincter muscle (bladder neck) 16 in order to determine and ensure the proper tension relationship between the tension-free vaginal tape 74 and the continence level being achieved by the urethral sphincter muscle 16 within the urethral canal 14.

Referring now to Figures 3 through 6, the urinary apparatus 10 operates in the following manner. In assembling the urinary apparatus 10, the flexible endoscope device 60 is received within a lumen 45 of the catheter system 40, such that the tip section 46 of the catheter system 40 is substantially aligned with the tip section 62 of endoscope device 60 (see Figure 3). As shown in Figure 3, the pressure gauge 48 and syringe member 50 are then connected at the proximal end of the catheter system 40, thereby allowing for the injection of fluid (i.e., a liquid or a gas) out of the tip section 46 from the attached syringe member 50. Additionally, the eye-scope member 64 and the video-monitoring scope member 68 are connected at the proximal end of the endoscope device 60.

The aligned tip sections 46 and 62 of the urinary apparatus 10 are then placed transurethrally within the urethral canal 14, such that the tip sections 46, 62

are positioned on the distal side of the external urethral sphincter muscle 16 adjacent to the bladder cavity 18 of the urinary system 12, as shown in Figure 4. The diameter of the catheter system 40 is slightly smaller than the natural diameter of the urethral canal 14 during high pressure bladder filling. To eliminate this condition, the obturator occlusion member 42 is slid into place in the urethral canal 14 to act as a luminal plug (see Figure 5). The catheter system 40 is now positioned in the urethral canal 14, such that the tip section 46 is positioned on the distal side of the urethral sphincter muscle 16 adjacent to the bladder cavity 18 and the obturator occlusion member 42 is positioned on the proximal side of the urethral sphincter muscle 16 adjacent to the urethral canal opening 14a, for pressurizing by fluid of the bladder cavity 18 in a manner which will be described hereinafter.

In order to pressurize the bladder cavity 18, fluid is added to the bladder to a level that is known to be comparable to the pressure experienced during thoracic muscular contracting (stress from coughing). By way of example, the fluid is added to a level as shown on pressure gauge 48 or pressure monitor 52 to a value of about 50mm Hg (as read off the gauge). The catheter system 40 is then retracted slightly, until the tip sections 46, 62 are repositioned on the proximal side of the closed urethral sphincter muscle 16 (see Figure 6), while the plug member 42 stays in place. This positioning maintains the bladder pressure of bladder cavity 18 and the firm placement of the plug member 42 within the urethral canal 14. Typically, after the repositioning of tip sections 46, 62 to the proximal side of the urethral sphincter muscle 16, the pressure level within the urethral canal 14 is now zero, as measured by pressure gauge 48 or 52.

The physician is now able to check and assess the tension-free vaginal tape (mesh) 74 for sling-tension (as described in U.S. Patent No. 5,899,909) by monitoring the orientation of the urethral sphincter muscle 16 via the video-monitoring scope member 68, as presented on the video monitor 70, or as shown through the eye-scope member 64. With reference to Figure 6, this assessment procedure is done by adding fluid and changing the applied fluid pressure, as shown by pressure gauge 48 or pressure monitor 52. More particularly, fluid is injected from the syringe member 50 and is filled into the urethral canal 14 in order to measure the

pressure for opening the urethral sphincter muscle 16 to induce reverse leakage back into the bladder cavity 18.

The physician is now able to perform an in-vivo urodynamic analysis for assessment of the positioning of the tension-free vaginal tape 74 about the urethral sphincter muscle 16. Under direct visualization by the physician, using the eye-scope member 64 or the video-monitoring scope member 68, the urethral support positioning of the tension-free vaginal tape 74 about the urethral sphincter muscle 16 may be adjusted in order to ensure the proper relationship between the tension-free vaginal tape 74 position and continence level as shown in Figures 7a, 7b and 7c.

Figure 7a depicts an in-vivo image indicating a fully opened urethral sphincter muscle 16 which shows no net effect on the incontinence level of the urethral canal 14, thereby indicating to the physician that the tension-free vaginal tape 74 is too loose in placement of the sling tape about the bladder neck of the bladder. This indicates to the physician that the tension-free vaginal tape 74 needs to be tightened about the urethral sphincter muscle 16 in order to restore continence to the urinary system 12.

Figure 7b depicts an in-vivo image indicating a fully closed urethral sphincter muscle 16 which shows that the placement and positioning of the tension-free vaginal tape (mesh sling tape) 74 has caused a complete and undesired closure of the urethral sphincter muscle 16 within the urethral canal 14. This indicates to the physician that the tension-free vaginal tape 74 is too tight and loosening of the tension-free vaginal tape 74 is therefore necessary in placement of the sling tape about the bladder neck in order to restore patency of the urethral sphincter muscle 16 by the physician.

Figure 7c depicts an in-vivo image indicating a partially closed urethral sphincter muscle 16 which gives a visualization of this urethral sphincter muscle 16 and the tension-free vaginal tape 74 being in a proper orientation.

The foregoing visualizations, as depicted by Figures 7a, 7b and 7c, allow the physician to apply fluid pressure (which may be altered) in order to simulate the effects of applied abdominal pressure to the bladder cavity 18 and to visually check on the effect of continence by the patient. This visualization shows the

physician that the tension-free vaginal (mesh) tape 74 was properly positioned relative to the bladder neck of the bladder (see Figure 6). The physician can now tighten or loosen the tension-free vaginal tape 74 ("tuning the tension-free vaginal mesh tape") by using the tip section 46 of the catheter system 40 on the tension-free vaginal tape 74 in which slack is tightened or removed from the tension-free vaginal tape 74. This tuning of the tension-free vaginal tape 74 is done repeatedly by the physician while repetitiously pressurizing, tensioning the mesh tape 74 and checking patency of the urethral sphincter muscle 16. The viewing of leakage flow ("trickle flow") is slowly and carefully acquired and visualized by the physician, allowing him or her to determine the point at which the urethral sphincter muscle 16 opens to achieve reverse leakage back into the bladder cavity 18 for a particular pressure level as depicted on pressure gauge 48 or pressure monitor 52. After the appropriate adjustment by the physician to the tension-free vaginal tape 74, the "opening pressure" of the newly repaired urethral sphincter muscle 16 may be checked by pressurizing the urethral sphincter muscle 16 from the bladder cavity 18 or from the outflow tract of the urethral sphincter muscle 16 within the urethral canal 14 in order to fill and check for leakage of the fluid in the bladder cavity 18.

During all of the catheter system 40 maneuverings and urethral pressurizing, the diameter of the urethral sphincter muscle 16 (under which the tension-free vaginal tape 74 is positioned), the inherent pressure of the bladder, and/or the urethral outflow tract are always measurable by the use of the urinary apparatus 10. If the tension-free vaginal tape 74 is observed to be too tight, a guide member (not shown) may be placed in the urethra after removing the urinary apparatus 10 at the site of the tension-free vaginal (mesh) tape 74. The guide member is pressed slightly in a downward direction to cause the tension-free vaginal tape 74 to be repositioned. This aforementioned adjustment procedure for the tension-free vaginal tape 74 is then repeated until the appropriate efficacy is achieved which allows the patient to restore continence with her bladder's micturition.

Bearing in mind that pressure ranges may vary from patient to patient and/or from physician to physician, let us assume that, for a particular hypothetical patient, the physician has determined that the appropriate sling tensioning level

corresponds to a pressure in a range of from about 22mmHg to about 48mmHg, which would indicate a proper orientation and positioning of the tension-free vaginal tape 74 about the urethral sphincter muscle 16. In the process of checking and tuning the tension-free vaginal tape 74 as depicted in Figure 6, the physician would

5 fill the urethral canal 14 with fluid in small increments from syringe member 50, while simultaneously checking the pressure level of the pressure gauge 48 or 52 to determine when the urethral sphincter muscle 16 opens as viewed in video-monitor 70. Let us further assume that the urethral sphincter muscle 16 opens at a pressure level of 10mmHg. Bearing in mind that the desired pressure range for sling

10 tensioning is between 22mmHg to 48mmHg, the pressure level reading of 10mmHg would indicate to the physician that the tension-free vaginal tape 74 is too loose and needs to be tightened.

After tightening of the tension-free vaginal tape 74 as described above, the physician would again fill the urethral canal 14 with fluid in small increments from

15 syringe member 50, while simultaneously checking the pressure level of the pressure gauge 48 or 52 to determine when the urethral sphincter muscle 16 opens as viewed in video-monitor 70. In this instance, let us assume that the urethral sphincter muscle 16 now opens at a level of 60mmHg. Again, bearing in mind that the desired pressure range for sling tensioning is between 22mmHg to 48mmHg, the pressure

20 level reading of 60mmHg would indicate to the physician that the tension-free vaginal tape 74 is too tight and needs to be loosened.

After loosening of the tension-free vaginal tape 74 as described previously, the physician once again fills the urethral canal 14 with fluid in small increments from syringe member 50, while simultaneously checking the pressure

25 level of the pressure gauge 48 or 52 to determine when the urethral sphincter muscle 16 opens as viewed in video monitor 70. Assuming the physician determines that the urethral sphincter muscle 16 now opens at a level of 38mmHg, this would indicate that the sling tensioning of the tension-free vaginal tape 74 is at a proper level of efficacy for providing continence to the patient for her bladder's micturition.

30 Referring now to Figures 9 and 10, there is shown another exemplary embodiment of a catheter system 80 adapted for use in combination with the endoscope device 60 of Figure 1, thereby forming a modified urinary apparatus 10'.

The catheter system 80 includes a fixed balloon occlusion member 82 used to inflatably block the urethral canal 14 in a manner similar to the obturator occlusion member 42 of Figure 2. The catheter system 80 has a proximal end which further includes a first inlet fill port 84 for receiving a fluid used to pressurize the bladder cavity 18 (as previously described), and a second inlet fill port 86 for receiving a fluid (liquid or gas) used to inflate and expand the fixed balloon occlusion member 82 with the urethral canal 14 of the urinary system 12. The fixed balloon member 82 is sized and shaped to fit the entrance opening 14a of the urethral canal 14 and is made from an expandable material. As shown in Figure 10, the catheter system 80 includes an endoscope lumen (opening) 88 for receiving the endoscope device 60 therein, a pressurization lumen 90 for receiving the fluid from the first inlet fill port 84, and a pair of balloon actuation lumens 92, 94 for receiving liquid or gas from the second inlet fill port 86.

With reference to Figures 9 and 10, the urinary apparatus 10' operates in exactly the same manner as the urinary apparatus 10 (see Figure 6), except that the fixed balloon occlusion member 82 is inserted and appropriately positioned within the urethral canal 14. The balloon member 82 is then expanded by liquid or gas from inlet fill port 86 via the balloon actuation lumens 92, 94 of catheter system 80. The physician now proceeds to operate the urinary apparatus 10' as fully described above in connection with the embodiment of Figures 1 through 6.

With reference to Figure 11, there is shown yet another exemplary embodiment of a catheter system 100 adapted for use in combination with the endoscope device 60 of Figure 1, thereby forming another modified urinary apparatus 10". The catheter system 100 includes a sliding balloon occlusion member 102 that inflatably blocks the urethral canal 14 in a manner similar to the fixed balloon occlusion member 82 of Figure 9. The sliding balloon member 102 is sized and shaped to fit the entrance opening 14a of the urethral canal 14 and is made from an expandable material. Additionally, the catheter system 100 has a proximal end which includes a first inlet fill port 104 for receiving a fluid used to pressurize the bladder cavity 18 (as previously described). The sliding balloon occlusion member 102 also has a proximal end which includes a second inlet fill port 106 for receiving fluid material (liquid or gas) therethrough for inflating and expanding

the sliding balloon occlusion member 102 within the urethral canal 14 of the urinary system 12. Further, the sliding balloon occlusion member 102 is moveable along a length of the shaft 108 of the catheter system 100.

Still referring to Figure 11, the urinary apparatus 10" operates in
5 exactly the same manner as the urinary apparatus 10 (see Figure 6), except that the balloon occlusion member 102 is slidably inserted and appropriately positioned within the urethral canal 14. The balloon member 102 is then inflated/expanded by liquid or gas from inlet fill port 106 of catheter system 100. The physician now proceeds to operate the urinary apparatus 10" as described above in connection with the
10 embodiment of Figures 1 through 6.

It should also be understood that the embodiments described herein are merely exemplary and that a person skilled in the art may make many variations and modifications without departing from the spirit and scope of the invention. For instance, pressure can be supplied to the bladder cavity 18 and the urethral canal
15 14 by means of a hydrostatic pressure head, such as a hanging fluid bottle/bag and an IV administration tubing set, which would replace the syringe member 50. In such a case, the applied pressure would still be measured by a suitable pressure gauge, such as an electronic pressure gauge or an analog tube gauge. All such variations and modifications are intended to be included within the scope of the invention as
20 defined in the appended claims.

What Is Claimed Is:

1. A urinary apparatus for assessing the sling tension of an implant support for restoring female urinary continence, comprising means for pressurizing
5 a bladder cavity and a urethral canal within a female urinary system; and means for observing a urethral sphincter muscle within the female urinary system for assessing the sling tension of the implant support.

2. A urinary apparatus in accordance with Claim 1, wherein said means
10 for pressurizing includes a catheter.

3. A urinary apparatus in accordance with Claim 2, wherein said catheter includes means for plugging the urethral canal so as to allow the pressurizing of the bladder cavity and the urethral canal.
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4. A urinary apparatus in accordance with Claim 3, wherein said means for plugging includes an obturator occlusion plug member slidably mounted on said catheter.

20 5. A urinary apparatus in accordance with Claim 4, wherein said plug member is sized and shaped to fit an entrance opening of the urethral canal and is made of solid and pliable plastic material.

6. A urinary apparatus in accordance with Claim 3, wherein said means
25 for plugging includes a balloon occlusion member, said balloon occlusion member being inflatable to a size and shape which fills an entrance opening of the urethral canal.

7. A urinary apparatus in accordance with Claim 6, wherein said balloon
30 occlusion member is slidably mounted on said catheter.

8. A urinary apparatus in accordance with Claim 6, wherein said balloon occlusion member is fixedly mounted on said catheter.

5 9. A urinary apparatus in accordance with Claim 2, wherein said catheter includes means for injecting a fluid into the bladder cavity and the urethral canal so as to allow the pressurizing of the bladder cavity and the urethral canal.

10 10. A urinary apparatus in accordance with Claim 9, wherein said means for injecting includes a syringe member.

11. A urinary apparatus in accordance with Claim 10, wherein said catheter includes means for measuring pressure of the bladder cavity and the urethral canal when receiving fluid from said syringe member.

15 12. A urinary apparatus in accordance with Claim 11, wherein said means for measuring pressure includes a pressure gauge.

20 13. A urinary apparatus in accordance with Claim 11, wherein said means for measuring pressure includes an electronic pressure gauge.

14. A urinary apparatus in accordance with Claim 2, wherein said means for observing includes an endoscope which is slidably received within said catheter.

25 15. A urinary apparatus in accordance with Claim 14, wherein said endoscope includes an eye-scope member.

30 16. A urinary apparatus in accordance with Claim 14, wherein said endoscope includes a video-monitoring scope member and a video monitor connected to said video-monitoring scope member.

17. A method for assessing the sling tension of an implant support for the urethral sphincter muscle of the bladder for restoring female urinary continence, comprising the steps of:

- 5 (a) pressurizing the bladder cavity with fluid to a predetermined pressure;
- (b) pressurizing the urethral canal with fluid to a pressure level at which the urethral sphincter muscle opens so as to induce reverse leakage back into the bladder;
- 10 (c) observing the opening of the urethral sphincter muscle during the performance of step (b); and
- (d) adjusting the sling tension of the implant support in response to the pressure level achieved during the performance of step (b).

18. A method in accordance with Claim 17, further comprising the
15 step of plugging the entrance opening of the urethral canal prior to the performance of step (a).

19. A method in accordance with Claim 18, further comprising the
step of selecting a desired pressure range for a particular patient, said desired
20 pressure range representing a desired sling tension of the implant support.

20. A method in accordance with Claim 19, further comprising the
steps of increasing the sling tension when the pressure level achieved during the
performance of step (b) is lower than said desired pressure range; and decreasing
25 the sling tension when the pressure level achieved during the performance of step
(b) is higher than said desired pressure range.

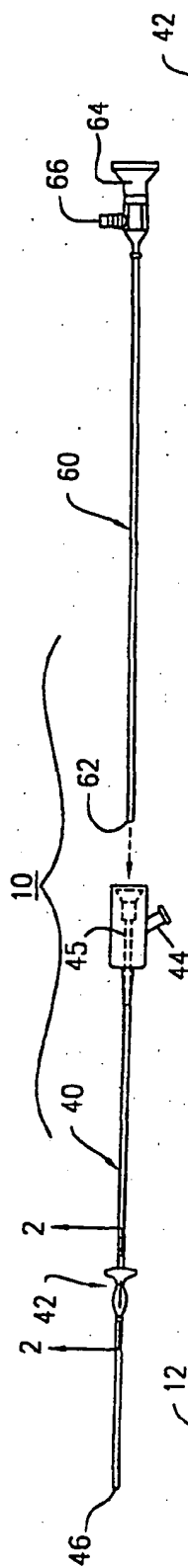


FIG. 1

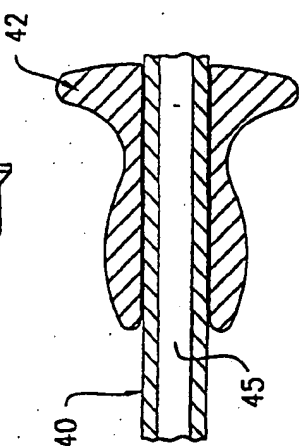


FIG. 2

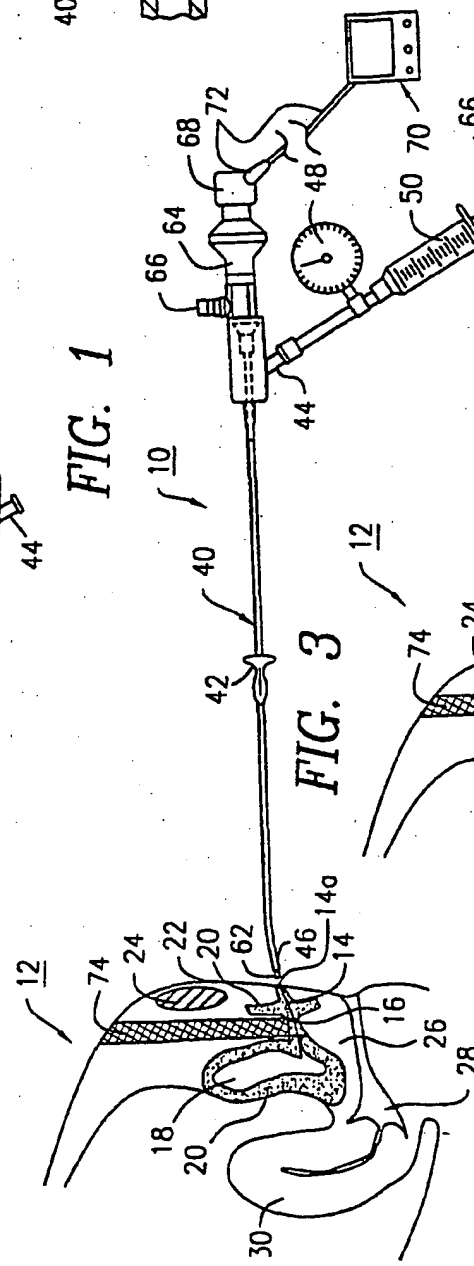


FIG. 3

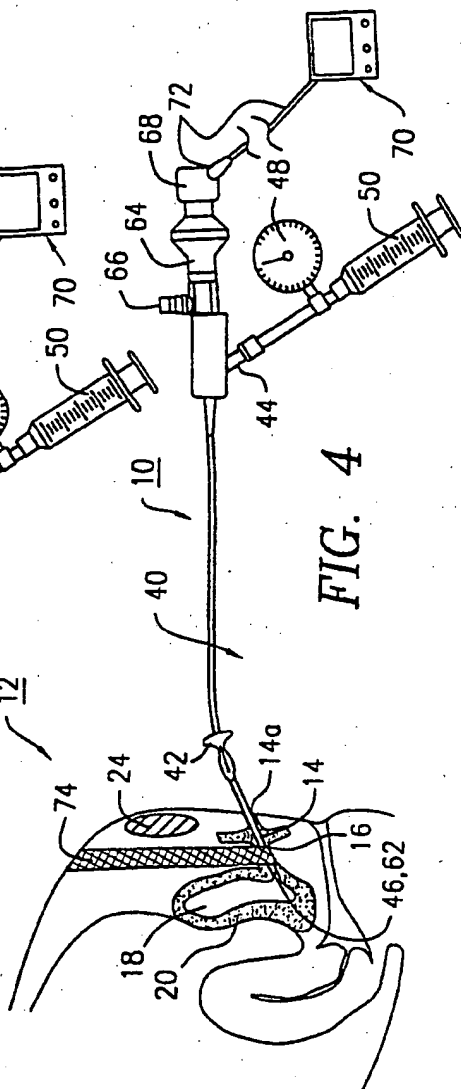
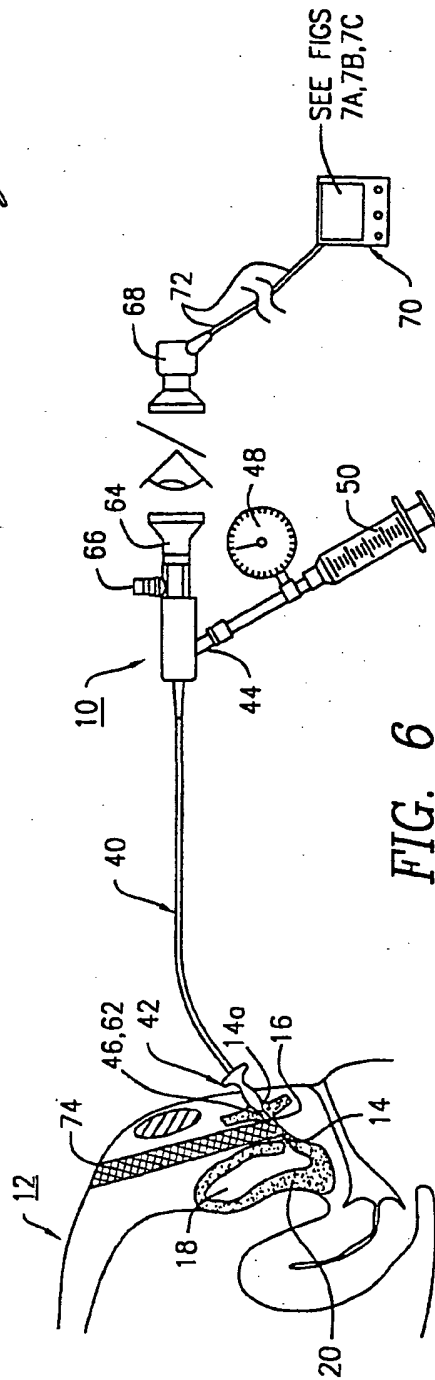
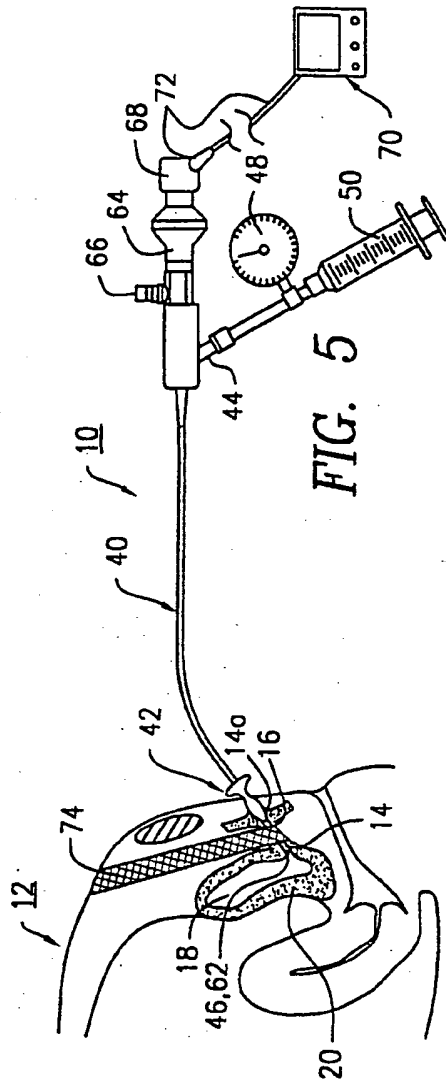


FIG. 4



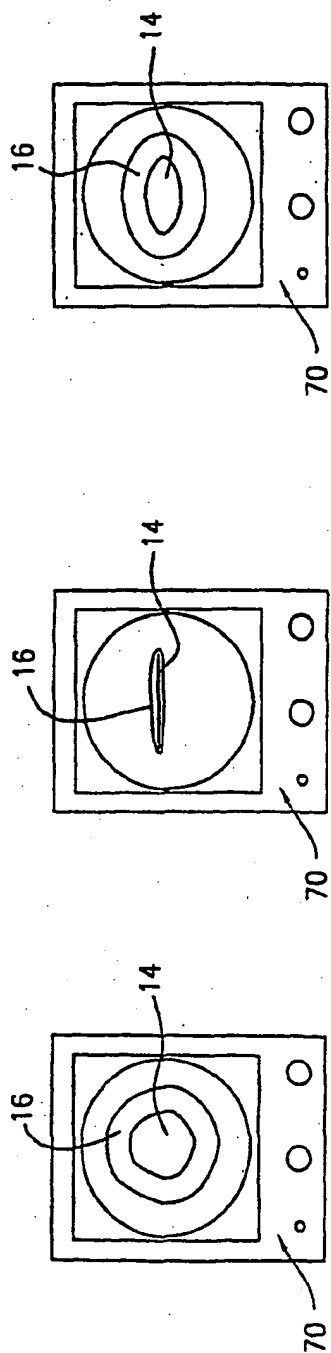


FIG. 7c

FIG. 7b

FIG. 7a

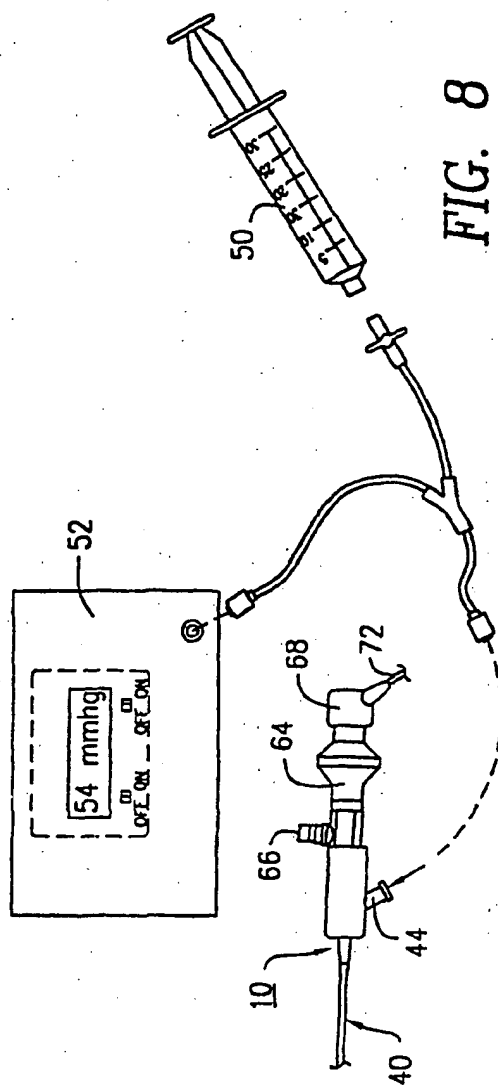


FIG. 8

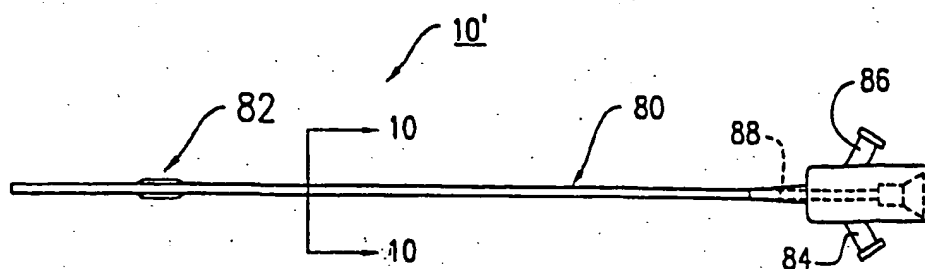


FIG. 9

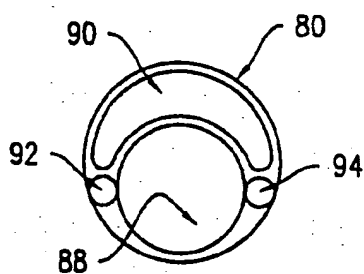


FIG. 10

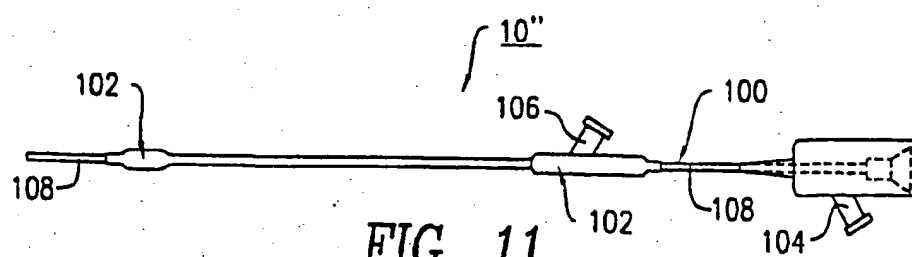


FIG. 11